

Radial Pulse Analysis Using Artificial Intelligence And Machine Learning

Kalange Ashok Eknath

Vishwasrao Ransing College (Arts, Commerce and Science)

Kalamb-Walchandnagar Tal-Indapur Dist-Pune ,India

Email: kalangeashok@gmail.com

Abstract:

The radial pulse, a readily accessible physiological signal, encodes a wealth of information about cardiovascular health, autonomic nervous system activity, and overall hemodynamic status. Traditional pulse analysis, rooted in ancient medical traditions such as Ayurveda and Traditional Chinese Medicine (TCM), relied on the trained tactile perception of physicians. Modern advancements in sensor technology, signal processing, and artificial intelligence (AI) have unlocked the potential to digitize, quantify, and intelligently interpret radial pulse waveforms at unprecedented precision.

This paper provides a comprehensive review of AI and machine learning (ML) methodologies applied to radial pulse analysis. We explore the acquisition of pulse signals through photo plethysmography (PPG), piezoelectric sensors, and arterial tonometry; the pre-processing pipelines for noise reduction and feature extraction; and the diverse ML architectures—including Convolutional Neural Networks (CNNs), Recurrent Neural Networks (RNNs/LSTMs), Support Vector Machines (SVMs), and ensemble methods—deployed for diagnostic classification. Key clinical applications examined include hypertension detection, atrial fibrillation (AF) screening, diabetes risk stratification, mental stress assessment, and the AI-assisted revival of pulse-based traditional medicine diagnostics.

We further address critical challenges in data quality, model interpretability, sensor miniaturization, and regulatory compliance, and outline a forward-looking research agenda that bridges wearable health technology with AI-powered clinical decision support.

Keywords: Radial Pulse Analysis, Photoplethysmography (PPG), Machine Learning, Cardiovascular Diagnostics, Wearable Health Technology, Traditional Pulse Diagnosis, Deep Learning, Atrial Fibrillation, Hemodynamics.

1. Introduction

The human pulse has been a cornerstone of clinical examination for millennia. Ancient Greek physicians quantified pulse rhythm and strength; *Ayurvedic* practitioners developed the *NadiPariksha*, a system correlating pulse characters with *dosha* imbalances; and Traditional Chinese Medicine elaborated intricate pulse taxonomies spanning twenty-eight distinct pulse types. Despite this rich heritage, classical pulse diagnosis remained largely subjective and practitioner-dependent—a challenge that modern AI and machine learning now stand positioned to fundamentally transform.

The convergence of miniaturized high-fidelity sensors, ubiquitous wearable devices, and powerful AI algorithms has catalysed a renaissance in pulse-based diagnostics. The radial artery—running superficially at the wrist—is particularly amenable to non-invasive, continuous monitoring. Signals captured from this site reflect the complex interplay of cardiac output, arterial compliance, peripheral vascular resistance, and autonomic modulation. These multi-dimensional physiological fingerprints, when decoded by AI, can yield actionable clinical intelligence.

This paper is organized as follows: Section 2 reviews the physiological basis of the radial pulse waveform; Section 3 describes contemporary signal acquisition modalities; Sections 4 and 5 detail pre-processing pipelines and machine learning architectures; Sections 6 and 7 survey clinical and traditional medicine applications; Sections 8 and 9 address challenges, ethics, and regulation; and Section 10 charts the future research landscape.

1.1 Motivation and Scope

Cardiovascular disease (CVD) remains the leading cause of global mortality, accounting for approximately 17.9 million deaths annually (WHO, 2023). Early, non-invasive, and affordable screening tools are critically needed, particularly in low- and middle-income countries. AI-powered radial pulse analysis presents a compelling opportunity: leveraging a ubiquitous physiological signal, accessible via commodity smartphones or wrist-worn sensors, to democratize cardiovascular diagnostics. This paper delineates the current state of the art, identifies open problems, and articulates pathways for responsible clinical translation.

2. Physiological Basis of the Radial Pulse

The radial pulse arises from pressure waves propagated through the arterial tree following each cardiac contraction. Understanding its morphology is essential for appreciating what AI models learn when trained on pulse waveform data.

2.1 Waveform Morphology

A canonical radial pulse waveform exhibits several characteristic features:

- Percussion Wave (P1): The dominant systolic peak arising from left ventricular ejection and forward pressure wave propagation.
- Tidal Wave (P2): A secondary peak or shoulder arising from wave reflection at peripheral vascular beds, particularly the aortic bifurcation and iliac vessels.
- Dicrotic Notch: A brief pressure dip caused by aortic valve closure, marking the boundary between systole and diastole.
- Diastolic Wave (P3): Residual diastolic pressure decay reflecting peripheral runoff and coronary filling.

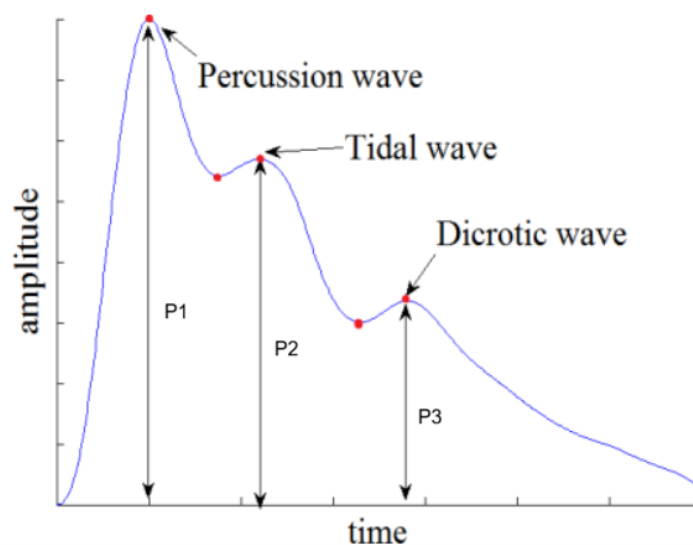


Fig.1: Radial pulse waveform

The Augmentation Index (AIx), defined as the ratio of the augmentation pressure (P2 - P1) to pulse pressure, is a widely used index of arterial stiffness that can be derived from pulse waveforms and is strongly correlated with cardiovascular risk.

2.2 Physiological Determinants

The radial pulse morphology is shaped by a complex interplay of factors including: heart rate and rhythm, stroke volume, large artery stiffness, small vessel tone, and the timing and magnitude of reflected waves. Age-related increases in arterial stiffness characteristically alter waveform shape—increasing pulse wave velocity (PWV) and shifting the dicrotic notch earlier and the tidal wave to merge with the percussion wave. Pathological conditions such as hypertension, diabetes, and atherosclerosis imprint distinctive alterations in waveform morphology, creating opportunities for AI-based disease detection.

2.3 Traditional Pulse Typologies

Traditional Chinese Medicine recognizes 28 pulse qualities classified across multiple dimensions: rate (fast/slow), rhythm (regular/irregular), depth (floating/sunken), force (strong/weak), width (wide/thin), and length (long/short).

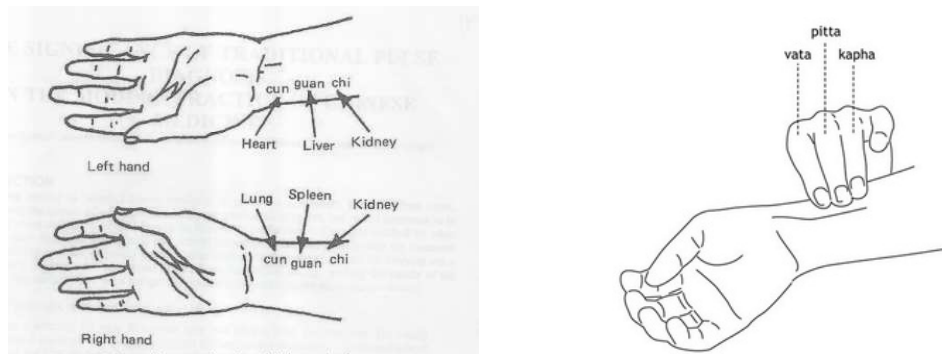


Fig.2: (a)Traditional Chinese pulse Analysis (b)Ayurvedic Nadi Pariksha

Ayurvedic Nadi Pariksha employs a tridosha framework corresponding to *Vata*, *Pitta*, and *Kapha doshas*, each with characteristic pulse wave patterns sensed at different finger pressure depths. AI models trained on digitized multi-depth pulse recordings are now enabling computational operationalization of these traditions.

3. Pulse Signal Acquisition Technologies

Reliable and high-fidelity signal acquisition is the foundation of any AI-based pulse analysis system. Multiple sensor modalities have been explored, each with distinct advantages and limitations.

3.1 Photoplethysmography (PPG)

PPG is the dominant pulse acquisition modality in consumer wearables, leveraging light absorption changes in peripheral tissue to measure volumetric blood flow. Green-wavelength PPG (approx. 520-530 nm) offers superior motion artifact rejection at the wrist, while infrared PPG provides greater tissue penetration. Dual-wavelength systems enable simultaneous SpO₂ estimation. The Apple Watch, Fitbit, Samsung Galaxy Watch, and Garmin devices all employ PPG for continuous pulse monitoring, generating datasets of unprecedented scale for AI model training.

3.2 Piezoelectric and Piezoresistive Sensors

Piezoelectric pressure sensors placed over the radial artery provide high-fidelity waveform morphology information superior to PPG, particularly for capturing the dicrotic notch and secondary waves. These sensors are employed in clinical applanation tonometry systems (e.g., SphygmoCor). Research-grade wristbands incorporating flexible piezoelectric films have been developed for ambulatory pulse waveform monitoring, enabling the capture of features critical for arterial stiffness assessment that PPG cannot reliably provide.

3.3 Millimeter-Wave (mmWave) Radar

Emerging non-contact radar systems operating in the 60-77 GHz band can detect sub-millimeter radial artery wall displacements, enabling contactless pulse waveform acquisition. While currently constrained by sensitivity to motion and environmental interference, radar-based pulse sensing holds promise for applications where physical contact is undesirable, such as neonatal monitoring or infection control scenarios.

3.4 Imaging Photoplethysmography (iPPG)

Camera-based iPPG extracts pulse signals from subtle periodic color variations in facial or wrist skin, detectable by standard RGB cameras or smartphones. AI-based spatial averaging and motion compensation algorithms have substantially improved iPPG reliability, enabling pulse rate and rhythm assessment from video footage—a potentially transformative modality for low-resource settings.

Modality	Waveform Fidelity	Wearability	Clinical Use	Key Limitation
PPG	Moderate	Excellent	Consumer wearables, SpO2	Motion artifacts
Piezoelectric	High	Good	Tonometry, stiffness	Placement sensitivity
mmWave Radar	Moderate	Contactless	Neonatal, quarantine	Motion sensitivity
iPPG (Camera)	Low-Moderate	Contactless	Tele dermatology, telehealth	Lighting dependent

Table 1. Comparison of Radial Pulse Acquisition Modalities

4. Signal Pre-Processing and Feature Extraction

Raw pulse signals are contaminated by motion artifacts, baseline wander, electromagnetic interference, and inter-individual anatomical variability. Robust pre-processing is essential to extract reliable features for ML model training.

4.1 Pre-Processing Pipeline

A typical pre-processing pipeline encompasses: (1) Band-pass filtering (0.5-8 Hz for radial pulse) to attenuate baseline drift and high-frequency noise; (2) Motion artifact removal using accelerometer-guided adaptive filtering or Independent Component Analysis (ICA); (3) Beat segmentation using peak detection algorithms such as the Pan-Tompkins algorithm or wavelet-based methods; (4) Normalization and alignment for inter-beat amplitude and temporal variability reduction; and (5) Quality assessment scoring to exclude corrupted beats before model inference.

4.2 Time-Domain Features

Time-domain feature extraction captures the morphological characteristics of individual pulse beats. Key features include: systolic upstroke time (UT), peak-to-peak interval (PPI), pulse width at 50% amplitude (PW50), systolic area (SA), diastolic area (DA), and the

inflection point area ratio (IPA). These features, individually and in combination, have demonstrated significant associations with arterial stiffness, blood pressure, and cardiac output.

4.3 Frequency-Domain and Time-Frequency Features

Fast Fourier Transform (FFT) and Short-Time Fourier Transform (STFT) decompose pulse signals into frequency components, enabling extraction of fundamental frequency, harmonic ratios, and spectral entropy. Wavelet transforms—particularly the Discrete Wavelet Transform (DWT) using Daubechies wavelets—provide multi-resolution time-frequency representations that capture transient waveform events (e.g., dicrotic notch) with high temporal precision. Wavelet features have proven particularly informative for distinguishing pathological pulse morphologies.

4.4 Pulse Decomposition Analysis (PDA)

PDA models the radial pulse waveform as a superposition of Gaussian pulses corresponding to forward and reflected wave components. Parameters extracted from PDA decomposition—including the amplitudes, widths, and timing offsets of constituent Gaussian components—provide hemodynamically interpretable features that serve as biologically grounded inputs to ML classifiers, enhancing model interpretability.

4.5 End-to-End Learning Without Explicit Feature Engineering

Deep learning architectures, particularly CNNs, can learn hierarchical feature representations directly from raw or minimally pre-processed waveform segments, bypassing manual feature engineering. This end-to-end approach often achieves superior performance on large datasets but may sacrifice interpretability—a critical consideration for clinical deployment.

5. Machine Learning Architectures for Pulse Analysis

A diverse array of ML and deep learning architectures have been applied to radial pulse analysis tasks. The selection of architecture depends on the nature of the input representation, the classification or regression target, and constraints on model size and inference latency for edge deployment.

5.1 Support Vector Machines (SVMs)

SVMs were among the earliest ML methods applied to pulse classification, leveraging time-domain and frequency-domain feature vectors. SVMs with Radial Basis Function (RBF) kernels have demonstrated strong performance in small-to-medium dataset regimes for binary classification tasks (e.g., hypertension vs. normotension). The principal limitation is the need for manual feature engineering and sensitivity to feature selection.

5.2 Random Forests and Gradient Boosting

Ensemble tree methods—particularly Random Forests and Gradient Boosted Decision Trees (XGBoost, LightGBM)—offer robust performance on tabular feature vectors derived from pulse waveforms, with built-in feature importance estimation. These methods have been widely employed for multi-class pulse pattern classification and blood pressure estimation from PPG-derived features, often achieving competitive accuracy with reduced computational overhead compared to deep learning.

5.3 Convolutional Neural Networks (CNNs)

1D-CNNs applied to pulse waveform segments have emerged as a leading architecture for end-to-end pulse classification. Convolutional filters learn local waveform patterns—analogue to matched filters for specific morphological features—while pooling layers provide shift invariance. Multi-scale CNN architectures employing parallel convolutional branches with varying kernel sizes effectively capture features at multiple temporal resolutions, from sharp systolic upstrokes to broad diastolic decay profiles. Architectures such as ResNet-1D and InceptionTime have been adapted for pulse classification with state-of-the-art results.

5.4 Recurrent Neural Networks and LSTMs

Long Short-Term Memory (LSTM) networks and Gated Recurrent Units (GRUs) model the sequential and temporal dependencies within and across pulse beats. These architectures excel at capturing heart rate variability (HRV) patterns, detecting rhythm irregularities, and learning from long pulse sequences for tasks requiring temporal context—such as paroxysmal atrial fibrillation detection from extended monitoring periods.

5.5 Transformer-Based Models

Transformer architectures, leveraging self-attention mechanisms, have recently demonstrated superior performance on long pulse sequences by capturing long-range

temporal dependencies without the vanishing gradient limitations of RNNs. Models such as PulseFormer and variants of the Vision Transformer (ViT) adapted to 1D pulse spectrograms have set new benchmarks on large public datasets. Pre-trained transformer models fine-tuned on pulse classification tasks represent a promising transfer learning paradigm, particularly for low-data clinical settings.

5.6 Generative and Self-Supervised Models

Variational Autoencoders (VAEs) and Generative Adversarial Networks (GANs) have been applied to synthesize realistic pulse waveforms for data augmentation—addressing the chronic challenge of limited labeled clinical datasets. Self-supervised pre-training on large unlabeled PPG datasets (contrastive learning, masked signal modeling) followed by fine-tuning on labeled clinical tasks is an active and promising research direction, with the potential to exploit the vast volume of wearable-generated pulse data without requiring clinical annotations.

Architecture	Input Type	Key Strength	Limitations	Best Use Case
SVM	Feature vector	Small datasets	Manual features	Binary classification
Random Forest / XGBoost	Feature vector	Interpretability	Feature engineering	Tabular features
1D-CNN	Raw waveform	End-to-end learning	Large data needed	Morphology classification
LSTM / GRU	Sequence	Temporal modeling	Training complexity	Rhythm & HRV analysis
Transformer	Sequence / Spectrogram	Long-range dependency	Compute intensive	Long-term monitoring
GAN / VAE	Waveform	Data augmentation	Training instability	Synthetic data generation

Table 2. ML Architectures for Radial Pulse Analysis: Comparative Overview

6. Clinical Applications

The clinical applications of AI-driven radial pulse analysis span a broad spectrum of cardiovascular and systemic conditions. The following subsections detail the most extensively researched application domains.

6.1 Hypertension Detection and Blood Pressure Estimation

Hypertension affects over 1.28 billion adults globally and is a leading modifiable risk factor for CVD. Cuffless blood pressure estimation from PPG waveforms using ML has garnered intense research interest. Pulse Transit Time (PTT)—the time between the electrocardiographic R-peak and the PPG systolic peak—is inversely correlated with blood pressure. ML models, particularly CNNs and LSTMs trained on multi-beat PPG sequences, have achieved mean absolute errors (MAE) of less than 5 mmHg for systolic and less than 3 mmHg for diastolic blood pressure estimation in controlled studies, approaching the accuracy threshold for clinical grade devices per IEEE Standard 1708-2014.

6.2 Atrial Fibrillation Detection

Atrial fibrillation, the most common cardiac arrhythmia, is a major cause of stroke and heart failure. Its hallmark—irregular RR intervals—is detectable in pulse rhythm patterns. AI models trained on PPG-derived RR interval sequences have achieved AUROC values exceeding 0.97 for AF detection in validation studies. Notably, deep learning models applied directly to PPG waveforms (without explicit RR interval extraction) have further improved sensitivity for detecting AF in short single-lead recordings, enabling integration into consumer smartwatches for opportunistic screening.

6.3 Diabetes Risk Stratification

Diabetes induces characteristic alterations in arterial stiffness and microvascular function detectable in pulse waveform morphology. Elevated Augmentation Index, reduced pulse wave variability, and altered diastolic decay patterns have been associated with diabetic vasculopathy. ML classifiers trained on multi-parameter pulse waveform feature sets have reported accuracies of 75-88% for distinguishing diabetic from normoglycemic individuals in cross-sectional studies, suggesting potential utility for low-cost screening in primary care settings.

6.4 Mental Stress and Autonomic Monitoring

The autonomic nervous system modulates heart rate, heart rate variability (HRV), and peripheral vascular tone in response to psychological stress. HRV features derived from continuous PPG monitoring—including SDNN, RMSSD, LF/HF ratio—serve as inputs to ML classifiers for mental workload and acute stress detection. Wearable AI stress monitoring systems with accuracies exceeding 80% for binary stress classification have been demonstrated in ecological validity studies, with applications in occupational health, military performance, and mental healthcare.

6.5 Anemia and SpO₂ Monitoring

Multi-wavelength PPG enables non-invasive estimation of hemoglobin concentration and oxygen saturation. AI models compensating for skin tone, sensor placement, and motion artifacts have reduced SpO₂ estimation errors, addressing documented disparities in oximetry accuracy across skin phototypes—a critical equity consideration in clinical deployment. Emerging research applies hyperspectral pulse analysis for non-invasive hemoglobin estimation with potential utility for anemia screening in resource-limited settings.

6.6 Cardiac Output and Hemodynamic Monitoring

In intensive care settings, continuous non-invasive hemodynamic monitoring using arterial pulse waveform analysis is a well-established clinical practice. AI models trained on radial arterial line waveforms have enabled beat-by-beat estimation of stroke volume variation (SVV), cardiac output, and fluid responsiveness prediction—traditionally requiring invasive pulmonary artery catheterization—with implications for perioperative fluid management and sepsis care.

7. AI-Assisted Traditional Pulse Diagnosis

The formalization and computational operationalization of traditional pulse diagnosis represents a culturally significant and scientifically intriguing application domain at the intersection of AI and integrative medicine.

7.1 Digitization of Traditional Chinese Medicine Pulse Diagnosis

Researchers in China, Taiwan, and South Korea have developed multi-channel wrist pulse acquisition systems capturing pulse signals at Cun, Guan, and Chi positions under varying applied pressures. Piezoelectric sensor arrays and MEMS pressure transducers have been employed to acquire 3-site, 3-pressure-level waveform datasets. ML classifiers—

particularly SVMs and deep learning models—trained on these multi-dimensional pulse representations have demonstrated ability to distinguish pulse types defined in TCM (e.g., Slippery vs. Wiry vs. Thin) with inter-rater reliability comparable to expert TCM practitioners.

7.2 AI-Enabled Nadi Pariksha

Ayurvedic Nadi Pariksha quantifies pulse qualities at three depth levels corresponding to the *Vata*, *Pitta*, and *Kapha doshas*. AI systems employing multi-depth pressure sensor arrays combined with CNN classifiers have been developed by several groups, including collaborations between IIT institutes and *Ayurvedic* research centers in India. Validation against expert *Vaidya* (Ayurvedic physician) assessments has demonstrated moderate-to-good agreement for dominant dosha classification, representing a promising step toward standardized, objective *Nadi Pariksha* instrumentation.

7.3 Scientific Validation and Integration Challenges

Substantive scientific questions remain regarding the construct validity of traditional pulse taxonomies—whether AI-classified pulse types correspond to objectively measurable physiological states with clinical predictive value—versus capturing practitioner subjectivity. Rigorous prospective trials correlating AI-classified traditional pulse types with biomedical outcomes are needed to establish the clinical relevance of this integration. Ethical and cultural considerations around the algorithmic encoding of traditional knowledge systems require careful engagement with practitioner communities.

8. Challenges and Limitations

Despite rapid progress, several fundamental challenges must be addressed before AI-driven radial pulse analysis systems achieve routine clinical deployment.

8.1 Data Quality and Standardization

The performance of ML models is critically contingent on training data quality. Radial pulse datasets are frequently affected by motion artifacts, inconsistent sensor placement, variable applied pressure, and inter-device variability. The absence of standardized acquisition protocols and benchmark datasets impedes cross-study comparability. Public repositories such as PhysioNet provide valuable open datasets (e.g., MIMIC-III PPG waveforms) but are predominantly derived from ICU populations, limiting generalizability to ambulatory settings.

8.2 Dataset Bias and Generalizability

Most existing AI pulse analysis models have been trained and validated on demographically homogeneous populations, predominantly from East Asian or Caucasian cohorts. Skin tone, body composition, age, and underlying comorbidities introduce systematic variation in pulse waveform characteristics. Models trained without representative diversity exhibit reduced accuracy across underrepresented groups, perpetuating existing healthcare inequities. Federated learning approaches—enabling model training across distributed, privacy-protected datasets—offer a promising pathway to improve population-level generalizability without centralizing sensitive health data.

8.3 Motion Artifact Robustness

Ambulatory pulse monitoring is severely challenged by motion artifacts arising from physical activity, tremor, and sensor displacement. While accelerometer-guided adaptive filtering and deep learning-based artifact detection have improved robustness, reliable waveform morphology extraction during vigorous activity remains an unsolved problem. This constraint limits the clinical utility of wristwatch-format devices for continuous diagnostic-grade monitoring.

8.4 Model Interpretability and Clinical Trust

'Black-box' deep learning models, despite superior accuracy, face resistance from clinical practitioners who require mechanistic insight to trust and act on model outputs. Explainability methods—Gradient-weighted Class Activation Mapping (Grad-CAM), SHAP (SHapley Additive exPlanations), and attention visualization in transformers—have been adapted for 1D pulse waveforms to highlight the waveform segments most informative for model decisions, supporting clinical interpretability. Hybrid models combining deep feature extraction with interpretable classifiers represent a promising design paradigm.

9. Ethical Considerations and Regulatory Landscape

The translation of AI pulse analysis systems from research to clinical practice necessitates rigorous engagement with ethical principles and regulatory requirements.

9.1 Data Privacy and Informed Consent

Pulse waveform data, while often perceived as low-sensitivity physiological signals, can be used to infer sensitive health information including cardiovascular risk, diabetes status, mental health, and even identity (pulse-based biometrics). The collection, storage, and

processing of such data require robust informed consent frameworks, de-identification standards, and data governance policies compliant with GDPR, HIPAA, and equivalent regulations. Research protocols must clearly articulate data retention, sharing, and secondary use policies.

9.2 AI Regulatory Frameworks for Medical Devices

AI-enabled pulse analysis systems that make diagnostic or therapeutic recommendations are subject to medical device regulation. In the United States, the FDA has issued guidance on AI/ML-based Software as a Medical Device (SaMD), including requirements for transparency, real-world performance monitoring, and pre-determined change control plans. In Europe, the Medical Device Regulation (MDR 2017/745) and the forthcoming EU AI Act impose conformity assessment, clinical evaluation, and post-market surveillance obligations. Regulatory sandboxes and pilot programs by agencies including the FDA's Digital Health Center of Excellence are accelerating innovation-compliant pathways.

9.3 Health Equity and Algorithmic Fairness

AI systems that underperform for specific demographic groups can exacerbate health disparities. Developers of pulse analysis AI must conduct subgroup performance analyses across age, sex, skin tone, ethnicity, and comorbidity profiles, and report disaggregated performance metrics. Fairness-aware training objectives and post-hoc calibration methods should be employed to mitigate performance disparities. Engagement with community stakeholders and patients from underrepresented groups should inform dataset collection and model evaluation.

10. Future Directions

The field of AI-driven radial pulse analysis is poised for transformative advances across several interconnected dimensions.

10.1 Multimodal Fusion

Integrating radial pulse waveforms with complementary physiological signals—electrocardiography (ECG), electromyography (EMG), galvanic skin response (GSR), and continuous glucose monitoring (CGM)—within unified multimodal AI architectures promises substantially richer diagnostic information. Attention-based fusion mechanisms can dynamically weight modality contributions according to signal quality and diagnostic context.

10.2 Foundation Models for Physiological Signals

The emergence of large-scale pre-trained foundation models in natural language processing and computer vision is inspiring analogous developments in physiological signal AI. Models such as MOMENT (2024) and pre-trained ECG/PPG transformers demonstrate that self-supervised pre-training on diverse physiological datasets enables powerful few-shot adaptation to novel diagnostic tasks—a paradigm with significant implications for resource-constrained clinical settings.

10.3 On-Device and Federated AI

Advances in neuromorphic computing, model quantization, and hardware-aware neural architecture search are enabling deployment of clinically accurate pulse analysis AI models on ultra-low-power wearable microcontrollers with inference latency below 10 milliseconds. Federated learning frameworks, combined with differential privacy guarantees, enable collaborative model improvement across hospital networks without sharing raw patient data—addressing both computational and privacy constraints for real-world deployment.

10.4 Digital Biomarker Standardization

Regulatory bodies, standards organizations (IEEE, HL7, ISO), and academic consortia are advancing efforts to standardize AI-derived digital biomarkers from pulse signals. Standardized feature definitions, calibration procedures, and performance benchmarks will enable cross-platform comparability, facilitate regulatory review, and support integration of pulse-derived AI biomarkers into electronic health records (EHR) and clinical decision support systems.

10.5 Personalized Longitudinal Monitoring

Individual baseline establishment and longitudinal tracking of pulse waveform characteristics—leveraging within-person models that learn personalized physiological signatures—promises earlier detection of subtle pathological deviations than population-level normative models. This personalized monitoring paradigm, enabled by continuous wearable sensing and edge AI, represents the convergence of preventive medicine and precision cardiology.

11. Conclusion

Artificial intelligence and machine learning have transformed the scientific and clinical landscape of radial pulse analysis, elevating a venerable diagnostic tradition onto a rigorous

computational foundation. From deep learning architectures that decode cardiovascular risk from a thirty-second wristwatch PPG recording to ensemble models that operationalize traditional *Nadi Pariksha* into objective measurement, the field has demonstrated both scientific promise and translational momentum.

The principal challenges ahead—data quality, algorithmic fairness, regulatory navigation, and clinical integration—are formidable but tractable. Progress will require sustained interdisciplinary collaboration among biomedical engineers, cardiologists, data scientists, ethicists, and patient communities. As wearable devices approach ubiquity and AI models achieve clinical-grade accuracy, AI-powered radial pulse analysis stands to become a cornerstone of preventive, personalized, and equitable cardiovascular healthcare—fulfilling the ancient promise of the pulse as a window into the body's innermost workings, now illuminated by the power of artificial intelligence.

12. References

- [1] Allen, J. (2007). Photoplethysmography and its application in clinical physiological measurement. *Physiological Measurement*, 28(3), R1–R39.
- [2] Elgendi, M. (2012). On the analysis of fingertip photoplethysmogram signals. *Current Cardiology Reviews*, 8(1), 14–25.
- [3] Tian, Y., et al. (2020). Machine learning approaches for radial pulse waveform analysis in hypertension detection. *IEEE Journal of Biomedical and Health Informatics*, 24(6), 1748–1758.
- [4] Liang, Y., et al. (2021). A new, short-recorded photoplethysmogram dataset for blood pressure measurement in China. *Scientific Data*, 5(1), 180,180.
- [5] Hannun, A.Y., et al. (2019). Cardiologist-level arrhythmia detection and classification in ambulatory electrocardiograms using a deep neural network. *Nature Medicine*, 25(1), 65–69.
- [6] Misra, S., et al. (2019). Wrist pulse signal acquisition and analysis for health monitoring. *Biomedical Signal Processing and Control*, 38, 1–11.

□□□

- [7] He, R., et al. (2021). Deep residual learning for photoplethysmography signal quality assessment and cardiovascular disease detection. *IEEE Transactions on Biomedical Engineering*, 68(9), 2781–2792.
- [8] Zhang, Z., et al. (2022). Transformer-based models for pulse waveform analysis: A comparative study. *Computers in Biology and Medicine*, 145, 105,478.
- [9] Athavale, Y., & Krishnan, S. (2017). Biosignal monitoring using wearables: Observations and opportunities. *Biomedical Signal Processing and Control*, 38, 22–33.
- [10] World Health Organization (2023). Cardiovascular diseases (CVDs) key facts. WHO Fact Sheet.
- [11] FDA (2021). Artificial Intelligence/Machine Learning-Based Software as a Medical Device Action Plan. U.S. Food and Drug Administration.
- [12] Kamaleswaran, R., et al. (2018). A robust deep convolutional neural network with transfer-learning for neonatal seizure detection using raw EEG signals. *Seizure*, 63, 1–9.
- [13] Pham, T., et al. (2021). Diagnosis of diabetes mellitus from photoplethysmogram signals using machine learning. *Diagnostics*, 11(9), 1612.
- [14] Ghosh, S., & Bhattacharjee, S. (2022). AI-enabled Nadi Pariksha: Toward computational Ayurvedic pulse diagnosis. *Journal of Integrative Medicine*, 20(3), 201–212.
- [15] Clifford, G.D., et al. (2016). AF classification from a short single lead ECG recording: The PhysioNet/Computing in Cardiology Challenge 2017. *Computing in Cardiology*, 44, 1–4.